Radiation Shielding Analysis and Optimisation for the MinPET Kimberlite Sorting Facility using the Monte Carlo Calculation Code, MCNPX

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Abstract. Radiation shielding calculations, analysis and optimization process carried out in order to design shielding for a Mineral-Positron Emission Tomography (MinPET) facility are presented. PET is a nuclear imaging technique commonly used in diagnostic medicine. The technique is based on the detection of 511 keV coincident and co-linear photons produced from the annihilation of a positron (produced by a positron emitter) and a nearby electron. This technique is currently being developed for mineral detection and quantification, particularly diamonds in kimberlite rocks through the MinPET facility. The facility is aimed at improving diamond mining through the early detection of the diamond bearing rocks. High energy photons are produced via bremsstrahlung when a high energy, 40 MeV 5mA, electron beam impinges on a high density target - tungsten. The resultant high energy photon beam is used to irradiate the candidate rock, activating the naturally occurring non-positron emitting isotope 12 C, producing a positron emitting isotope 11 C via a photo-nuclear (γ, n) reaction. The resultant high intensity and high energy radiation field (which includes both photons and neutrons up to 40 MeV) requires appropriate shielding to protect personnel and the environment around the facility. A Monte Carlo based radiation transport code, MCNPX, was used to model the MinPET facility including the electron accelerator, the irradiation chamber and the proposed shield. Shielding calculations were performed, applying the theory of interaction of radiation with matter together with the modeling and the radiation transport calculation capabilities of MCNPX. The calculations were applied to determine the types, optimum combinations and thickness of shielding materials. About 1.6 m of shielding composed of lead, iron, wax and boron carbide combined in the shield matrix were found to be sufficient to drop dose rates to acceptable levels on the personnel side of the shield, where several meters of concrete would have been required.

1. Introduction

MinPET is a revolutionary technology that is expected to improve diamond mining and sorting by introducing efficiency in the usage of equipment, energy and water. The technique is based on the detection of 511 keV coincident and co-linear photons produced from the annihilation of a positron (produced by a positron emitter) and a nearby electron. The technique is popularly used in diagnostic medicine and is now being developed for use in the mining sector and in particular the identification of diamond from kimberlite rocks. The current diamond extraction process involves the crushing of candidate rocks several times to small pieces, typically to a few

millimeters in diameter exposing the diamonds to the surface. Physical separation techniques are then applied to extract the diamond particles. It has been noted however, that only a small fraction of the crush actually contains significant quantities of diamond particles[1]. The crushing process is energy, equipment and water intensive.

In the MinPET technique, the rocks are only crushed to manageable sizes, equivalent to the "first crush". A high energy photon beam at least 23 MeV, is used to irradiate the rocks thus activating the naturally occurring, non-positron emitting ¹²C, producing a positron emitting ¹¹C via a photo-nuclear reaction namely 12 C(γ , n) 11 C. A 40 MeV electron beam, incident on a tungsten target is used to produce the high energy photon beam through bremsstrahlung.

The high energy photons, the resultant neutrons from the (γ, n) reaction and products from other $^{12}C(*,*)^{11}C$ processes due to the interaction of photon beam with rock constituents, the primary electrons from the accelerator and the γ -rays from resultant radioactive products all create a high energy, mixed radiation field in and around the MinPET facility. The need for an appropriate shield to protect personnel and the environment around the facility cannot be over emphasised.

A Monte Carlo radiation transport code, MCNPX was used to model the facility and together with radiation transport theory, calculations were carried out to developed an optimum shield for this facility.

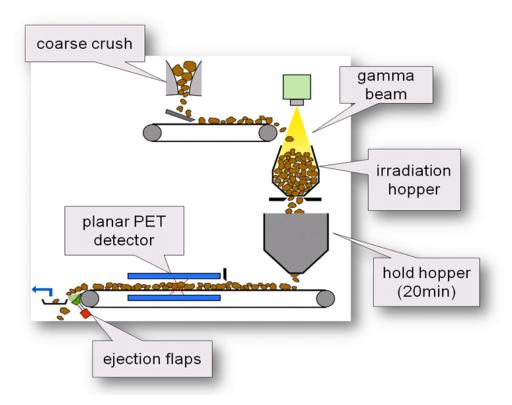


Figure 1. The MinPET process flow

2. The MinPET Facility

Figure 1 shows the process flow in the MinPET facility. Kimberlite rocks are coarse crushed, "the first crush", and carried by a conveyor belt to the irradiation chamber. A photon beam

is directed towards the irradiation chamber so that activation can take place. The activated rocks are then fed into a holding chamber where they are held for 20 mins, enough time to allow unwanted short lived activated products, which may interfere with the detection signal, to decay away. The proposed shield should cover the accelerator, the irradiation and the holding chambers, excluding the detection system. It has been determined that the irradiation process does not yield long lived activation products, hence it is not necessary at this stage to design a shield that covers the detection system. This reduces the cost of the shield. It must be noted at this stage, that a static system was modelled, due to MCNPX limitations. In reality, the rocks are continuously fed into the two chambers and into the detection system by the conveyor belts. However, this static system sufficiently approximates the dynamic system from a radiological point of view.

3. MinPET Facility simulation

MCNPX version 2.7.e with ENDF/B-7.0 cross-section data (2008) was used for the shielding calculations. First, a simple model of the facility was developed and the geometry was plotted using a graphic application, Vised X, for debugging purposes especially to check the relative positions of the irradiation chamber, the electron beam and the tungsten target.

4. Source Term Characterisation

The first step in the development of a shield is source term characterization. This process was carried out to determine the type of radiation sources and the energy distribution, including the respective directions of radiation particles. The results of the MinPET facility source term characterisation are shown in Figures 2 - 3. Figure 2 (left) shows the variation of photon flux with energy at different polar angles around the accelerator and Figure 2 (right) shows the variation of the photon flux with energy at different axial positions from the accelerator. A positive sign represents a position above the accelerator and negative means below. It is assumed here that the radiation produced, is symmetric around the azimuthal angle because the beam is un-polarised.

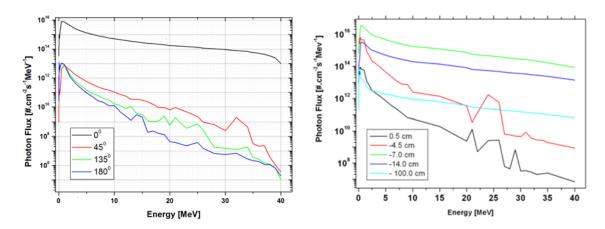
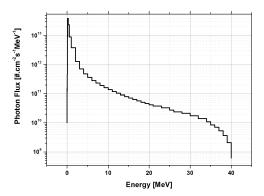


Figure 2. Photon flux at various polar angles and at different axial positions

A mesh tally was set up around the facility to further ascertain the levels of radiation dose produced by the MinPET and the mesh tally results are shown in figure 4.

5. Radiation Transport

Ionising radiation can be in the form of electrically charged particles such as alpha particles, beta particles, protons and heavy ions or uncharged particles and radiation quanta such as neutrons,



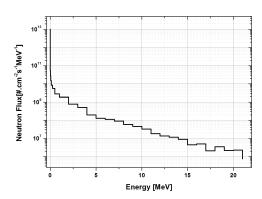
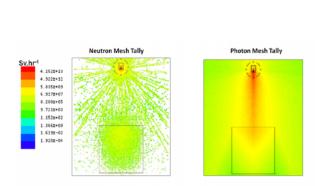


Figure 3. Total photon and neutron flux in the irradiation chamber



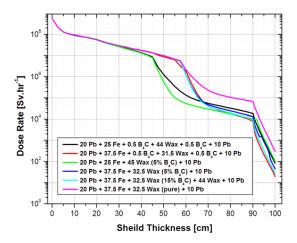


Figure 4. Neutron and photon mesh plots in the MinPET

Figure 5. Dose rates for six different shield configurations.

gamma radiation and X-rays [2]. Charged particles do not present major shielding problems because they lose large amounts of energy in each interaction as they interact with matter and as a result, charged particles are characterized by short ranges in matter [3]. However it is important to note that charged particles may produce secondary electromagnetic radiation i.e. bremsstrahlung photons, which contribute to the radiation field.

Neutrons and photons are the most difficult radiation types to shield and are therefore the center of focus in this paper. Neutral particles generally move between points of interaction in straight lines. Their mean free path (mfp) and hence the range of neutral ionising radiation is much longer than those of charged particles. Neutral particles cause ionisation indirectly and ultimately transfer their energy to charged particles which then cause the direct ionisation [4].

6. Interaction of Radiation with Matter

To design nuclear systems, one needs to understand the way in which radiation interacts with matter [5]. A study of neutron scattering kinematics and dynamics [6], [7], [8], [9], [10], [11] shows that the isotope ⁵⁶Fe has a high cross section for neutron inelastic scattering at high neutron

energies and the isotope 1H has a very high energy-lowering elastic scattering cross-section at relatively low neutron energies. Furthermore, the isotope 1H has a high cross-section for neutron capture, albeit with a subsequent production of highly ionising photons. Any neutron capture reaction (n, γ) , for that matter introduces secondary ionising photons. However the isotope, ^{10}B , produces very low energy photons in the $^{10}B(n, \alpha)^7Li$ reaction hence its introduction into the radiation shield helps to suppress the production of the high energy photons.

Ionising photons are "killed" off by using high atomic number Z and high density materials within the shield. A beam of monochromatic photons moving through an absorber (shield) displays a characteristic exponential reduction of the number of photons travelling along the original direction [7], [12].

7. Shielding Scheme

From the principles of neutron and photon shielding it can be seen that the effective and optimal shield should contain the following materials:

- (i) Lead to attenuate gamma rays (high Z, high ρ) and begin to slow down fast neutrons.
- (ii) **Iron** to attenuate high energy neutrons (via inelastic scattering).
- (iii) **Wax** to further attenuate and absorb neutrons slowed down by iron to within the cross-section group of ¹H (wax is rich in ¹H).
- (iv) Boron carbide (B_4C) used on its own or mixed with wax. The isotope ^{10}B suppresses the production of high energy secondary photons. Ammonium pentaborate can be used as alternative.

8. Shield Optimisation

Six different shield configurations were developed as detailed in figure 5. The graph shows the total dose rate as a function of distance from the internal surface of the shield to the external surface for each configuration. All six configurations show a considerable reduction of dose rates within 100 cm. Due to space constraints in the MinPET facility, the shield was restricted to about 100 cm.

By considering the results in figure 5 the best shield configuration in this study contains 20cm lead, 37.5 cm iron, 31.5 cm wax flanked by 0.5 cm strips of B_4C and finally 10 cm lead in laminar sheets.

9. Shield Effectiveness

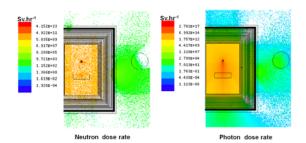
Figure 6 shows the reduction of neutron and photon dose rates hence the effectiveness of the selected shield configuration. It can been seen that the internal space has high dose rates, in the order of 10^{17} Svhr⁻¹ and in the external environment the dose rates go down, in the order of 10^{1} Svhr⁻¹ for photons and 10^{2} Svhr⁻¹ for neutrons.

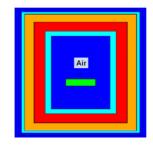
10. MinPET proposed shield

Figure 7 shows the proposed shield for the MinPET facility. The shield forms a 200 cm by 200 cm by 200 cm (internal dimensions) room with walls about 100 cm thick. Figure 7 (A) shows the full cross section of the room and Figure 7 (B) shows the cross-section of one side the shield wall.

11. Conclusions

The study shows that the operation of the MinPET activation system produces very high radiation doses around it and and a properly designed shield is a necessity. Although the proposed shield structure in figure 7 is very effective, it reduces the photon dose more





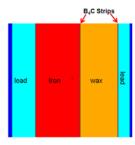


Figure 6. Mesh plots showing the reduction of **Figure 7.** Proposed Shield for the MinPET dose rates from the interior going out through Facility the shield

considerably, relative to neutron dose. Neutrons are more penetrating than photons with the same energy. The resultant dose given in section 9 above are still too high considering the annual dose limits prescribed in the ICRP [13],[14]. These are 1 mSv/year for the public and 20 mSv/year for regulated occupational exposure (this is effectively 20 μ Sv/hour for the latter case). Considering these minimum dose limits, the shield must be made somewhat thicker beyond the 100 cm limit considered here. This adjustment increases the cost of producing the shield but it will reduce the dose rates to the required few μ Sv/hour range.

12. Acknowledgments

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